Medical Image Analysis 17 (2013) 844-857

Contents lists available at SciVerse ScienceDirect

Medical Image Analysis

journal homepage: www.elsevier.com/locate/media



Tractometer: Towards validation of tractography pipelines

Marc-Alexandre Côté, Gabriel Girard, Arnaud Boré, Eleftherios Garyfallidis, Jean-Christophe Houde, Maxime Descoteaux*

Sherbrooke Connectivity Imaging Laboratory (SCIL), Computer Science Department, Université de Sherbrooke, Sherbrooke, Québec, Canada

ARTICLE INFO

Article history: Available online 25 April 2013

Keywords: Diffusion MRI Tractography Validation Connectivity analysis

ABSTRACT

We have developed the *Tractometer*: an online evaluation and validation system for tractography processing pipelines. One can now evaluate the results of more than 57,000 fiber tracking outputs using different acquisition settings (*b*-value, averaging), different local estimation techniques (tensor, q-ball, spherical deconvolution) and different tracking parameters (masking, seeding, maximum curvature, step size). At this stage, the system is solely based on a revised FiberCup analysis, but we hope that the community will get involved and provide us with new phantoms, new algorithms, third party libraries and new geometrical metrics, to name a few. We believe that the new connectivity analysis and tractography characteristics proposed can highlight limits of the algorithms and contribute in solving open questions in fiber tracking: from raw data to connectivity analysis. Overall, we show that (i) averaging improves quality of tractography, (ii) sharp angular ODF profiles helps tractography, (iii) seeding and multi-seeding has a large impact on tractography outputs and must be used with care, and (iv) deterministic tractography produces less invalid tracts which leads to better connectivity results than probabilistic tractography.

© 2013 Elsevier B.V. All rights reserved.

1. Introduction

Diffusion MRI and fiber tractography have gained importance in the medical imaging community for the last decade. The neuroscience community often uses fiber tractography as a black box, and its limits are ignored by most. The diffusion community has done a good job in the last years to highlight the limitations of diffusion tensor imaging (DTI) (Descoteaux et al., in press) in crossings and high curvature areas. Thus, numerous new high angular resolution diffusion imaging (HARDI) tractography techniques have been proposed (Descoteaux, 2008; Seunarine and Alexander, 2009; Descoteaux et al., in press). Most of these HARDI techniques have been

* Corresponding author. Address: Computer Science Department, 2500 Boulevard Université, Sherbrooke, Québec, Canada J1K 2R1. Tel.: +1 819 821 8000x66129; fax: +1 819 821 8200.

E-mail address: m.descoteaux@usherbrooke.ca (M. Descoteaux).

1361-8415/\$ - see front matter @ 2013 Elsevier B.V. All rights reserved. http://dx.doi.org/10.1016/j.media.2013.03.009 tested quantitatively on the sharpness of the peaks (angular resolution) and accuracy of the orientation distribution function (ODF) reconstruction based on simulated data. In neurosurgery, quantitative evaluation of fiber tracking results has been done by comparing tracts to electrocortical stimulation points (Kinoshita et al., 2005), or by measuring patient outcomes given the use of tractography for the resection of tumors (Wu et al., 2007; Spena et al., 2010). However, the comparison between tractography algorithms remains mainly qualitative for the most part. Most often, fiber tracking results are shown on major fiber bundles such as the corticospinal tract (CST), the corpus callosum (CC), superior longitudinal fasciculus (SLF), cingulum (Cg) and inter-hemispheric projections able to connect the left and right hemispheres. Several groups have studied the effect of interpolation (Tournier et al., 2012; Dyrby et al., 2011), step size (Tournier et al., 2011; Tournier et al., 2012; Sotiropoulos, 2010), stopping criteria (Girard and Descoteaux, 2012; Girard et al., 2012; Smith et al., 2012a; Smith et al., 2012b; Guevara et al., 2011; Garyfallidis, 2012), but mostly qualitatively on major fiber bundles.

Validation of fiber tractography remains an open question and a challenge on real data. Good reviews can be found in (Hubbard and Parker, 2009) and in (Fillard et al., 2011), where synthetic phantom data (Perrin et al., 2005; Fieremans et al., 2008; Pullens et al., 2010; Bach et al., 2011; Moussavi-Biugui et al., 2011), histological data (Leergaard et al., 2010; Anderson et al., 2006; Dauguet et al., 2007; Budde and Frank, 2012), biological *ex vivo* phantom data



Abbreviations: a-ODF, Analytical Orientation Distribution Function (ODF); ABC, Average Bundle Coverage; CC, Corpus Callosum; Cg, Cingulum; csa-ODF, Constant Solid Angle ODF; CSF, Cerebral Spinal Fluid; CST, Corticospinal Tract; dMRI, diffusion Magnetic Resonance Imaging; DTI, Diffusion Tensor Imaging; DWI, Diffusion Weighted Imaging; fODF, Fiber ODF; FA, Fractional Anisotropy; GM, Grey Matter; HARDI, High Angular Resolution Diffusion Imaging; IB, Invalid Bundles; IC, Invalid Connections; ODF, Orientation Distribution Function; NC, No Connections; r6, maximal SH order 6; rk, Runge–Kutta; ROI, Region Of Interest; SD-r6, Spherical Deconvolution of maximal SH order 6 (r6); SLF, Superior Longitudinal Fasciculus; TEND, Tensor Advection; VB, Valid Bundles; VC, Valid Connections; WM, White Matter.



Fig. 1. FiberCup mimicking a coronal slice of the brain with typical short 'U' fibers (bundle 4), larger 'U' fibers mimicking the corpus callosum (bundle 1), left-to-right hemisphere commissural projections (bundle 3) and fanning bundles mimicking the corticospinal tract (bundles 2, 5, 6 and 7).



Full streamline output

Valid connections and bundles

Fig. 2. Example of a tractography pipeline output and the resulting valid connections filtered by the ROIs.

(Campbell et al., 2006), and numerical simulation data (Hall and Alexander, 2009) are detailed.

Recently, the FiberCup phantom dataset (Fillard et al., 2011) was proposed to study the effect of the huge variety of diffusion models. tractography and combinations thereof. This phantom is publicly available (www.lnao.fr/spip.php?article112) and is now used by the community for quantitative evaluation of tracking algorithms (Pontabry and Rousseau, 2011; Reisert et al., 2011; Wilkins et al., 2012b; Wilkins et al., 2012a; Röttger et al., 2011; MomayyezSiahkal and Siddiqi, 2010). However, the original FiberCup contest does not well reflect brain connectivity analysis, especially in terms of seeding and performance evaluation. In our opinion, two important drawbacks of the FiberCup are the placement of the seed points given and the quantitative metric used to compare with ground truth. Only 16 seeds are given and these are close to boundaries and in the middle of structures. These 16 seeds result in 16 individual streamlines that are compared with the ground truth in terms of spatial, tangent to the tract and curvature distances. These measures are local and do not capture well the global connectivity profile of the tractography algorithm. Other problems are that each participant of (Fillard et al., 2011) performed his own analysis and that the implementations used are not available to the community.

In this paper, we propose a revised FiberCup analysis that is closer in spirit to brain connectivity analysis. In brain connectivity, the importance is *connectivity*. Does region A connect to B as expected? Does region A connect to unexpected regions of the brain? Therefore, instead of using local seeds and local point-by-point distances for evaluation, we propose a global view of the dataset and the fiber tractography streamline output. We developed an evaluation method to compare tractography pipeline streamline outputs and evaluate the number of *found* and *not found* fiber bundles, the proportion of streamlines part of existent and non-existent bundles, and the proportion of incomplete streamlines. Since these characteristics have a direct impact on connectivity analysis, having a tractography evaluation tool is crucial for human connectome studies.

This paper is thus aimed at providing a framework to encourage the community to rigorously choose a tractography processing pipeline and report the known limitations of their technique. Therefore, in the rest of the paper, we describe our new online system to evaluate and rank pipelines (url: tractometer.org). At this stage, a user has the choice of providing 3 things to the system: (1) A diffusion dataset corrected with the user's best algorithm, (2) a field of ODFs coming from the user's best algorithm, or (3) a set of streamlines. The user can then obtain a ranking against the current database of state-of-the-art techniques. Presently, in this database, we have N = 57,096 different streamline outputs of tractography pipelines coming from our in-house tools, MRtrix (Tournier et al., 2012) and TrackVis (Diffusion Toolkit) (trackvis.org) using the different FiberCup acquisitions, local estimation techniques, and tracking parameters. A preliminary version of this paper appears in the MICCAI 2012 proceedings (Côté et al., 2012). Relative to that contribution, the current work adds 56,000 tractography pipelines to the testing framework, including new datasets of different *b*-values and new tractography algorithms. We also added new quantitative connectivity measures.

2. Materials and methods

2.1. Terminology

The diffusion MRI community needs to agree on definitions for fiber tracking. Unfortunately, there are many examples of confusing and contradictory definitions used in the literature and used by clinicians, researchers and laboratories. Here, we make several suggestions and define the terms used in this paper. We first separate our terms in three sections: (i) general terms, (ii) terms that concern anatomy and (iii) terms that concern imaging.

General. Fiber: a long and thin structure. Hence, fiber tracking is a general term that can be used in any field that reconstructs fibrous structures, such as hair fibers, celery fibers, muscle fibers, prostate fibers, brain fibers, etc.

Brain Anatomy. Axon: the long fiber-like part of a nerve cell along which impulses are conducted from the cell (μ m scale). Tract: a group of neuronal axons in the central nervous system (mm scale). Fiber bundle: a group of fibers usually with an anatomical or functional meaning, e.g. arcuate fasciculus, fornix, etc. A *fiber bundle* for the area of brain anatomy is synonymous to a *tract*, also often called *fiber tract*. The term tract can be misleading when talking for example about the corticospinal tract. The corticospinal tract is not a single tract but a group of tracts.

Brain Imaging. Streamline: an imaginary line approximating the underlying fiber. *Streamlines bundle*: a group of streamlines with similar shape and spatial characteristics. These do not necessarily correspond to individual fiber bundles. *Tractography*: the process of generating streamlines of brain fibers. This is synonymous with fiber tracking in the central nervous system.

2.2. A revised FiberCup analysis

Fig. 1 illustrates the FiberCup dataset mimicking a coronal slice of the human brain. The phantom was built following the procedure of (Poupon et al., 2008; Poupon et al., 2010) for the MICCAI FiberCup workshop held in 2009, which resulted in a tractography comparison paper in (Fillard et al., 2011). Note that streamlines are colored using the rgb (red–green–blue) convention throughout the paper, i.e. red streamlines for left–right and green for top-down streamlines. Since the FiberCup is a 2D axial dataset, there are no blue streamlines coming out of the page. This also means that the connections mimicking the CST are actually green in the FiberCup dataset as opposed to the normal blue color in a classical brain rgb map.

In our opinion, the metrics proposed in (Fillard et al., 2011) are too local and vulnerable to the seeds given and, as a result, do not capture the global *connectivity* behavior of the fiber tracking algorithm. To better reflect brain connectivity studies, especially in terms of seeding and performance evaluation, we revisit the Fiber-Cup analysis. The main difference is to consider two different starting configurations: (1) From a complete mask of the phantom mimicking a brain white matter (WM) mask, as seen in Fig. 7, or (2) from ROIs mimicking gray/white matter interfaces, as seen in Fig. 7. Hence, the output streamlines from a tractography algorithm, such as those shown in Fig. 2 (left), can be filtered by the ROIs at the end of bundles (Fig. 7, middle-left) to quantify the global success and errors present in tractography output. Hence, we propose new connectivity metrics highlighting the global errors and success rate of tractography pipelines.

2.2.1. Definitions and rationale

We performed a survey with neurosurgeons and neurologists at our institute concerning true and false connections, and false positives of streamlines. We concluded that these terms were not the best choices for connectivity analysis purposes. Therefore, we define the following six new terms:

• Average Bundle Coverage (ABC): the proportion of a fiber bundle covered by streamlines. ABC is reported in % (percentage) and is the average of the number of voxels crossed by streamlines divided by the total number of voxels in the bundle. For

example, in Fig. 2, bundles 4, 6 and 7 have a high ABC, whereas bundle 3 has a much lower ABC.

- Valid Connections (VC): streamlines connecting expected ROIs and not exiting the expected fiber bundle mask. This is illustrated by streamlines in Fig. 2 (right). VC will be reported in % of valid connections.
- *Invalid Connections (IC)*: streamlines connecting unexpected ROIs or streamlines connecting expected ROIs but exiting the expected fiber bundle mask. These streamlines are spatially coherent, have managed to connect ROIs, but do not agree with the ground truth (see Fig. 3). IC are reported in %. According to our survey with clinicians, these are the most problematic streamlines as they "appear plausible" (because for example they connect gray matter regions) but are in fact non-existent from *a priori anatomical* knowledge.
- *No Connections (NC)*: streamlines that do not connect two ROIs. Depending on how fiber tracking handles stopping criteria, these streamlines either stop prematurely due to angular constraints or, most often, due to hitting the boundaries of the tracking mask, as illustrated in Fig. 4.
- *Valid Bundles (VB)*: bundles connecting expected ROIs. Fig. 1 (left) shows the valid bundles. VB is reported in bundle counts, from 0 to 7 for the FiberCup. For example, in Fig. 2, VB = 7.
- Invalid Bundles (IB): bundle connecting unexpected ROIs. As VB, IB is reported in bundle counts and is similar to IC, but at the bundle scale. For example, this is shown in Fig. 3, where bundles 1, 3 are mismatched. However, note that they "look anatomically plausible", had we not known the ground truth. In theory, there are a total of 39 possible IB.

2.3. Overview of tractography pipelines currently part of the Tractometer

Acquisition. There are three acquisitions with different *b*-values available in the current version of the Tractometer, corresponding to the *b* = 650 s/mm², *b* = 1500 s/mm² and *b* = 2000 s/mm² datasets shown in Fig. 5. For each acquisition, there were 64 uniformly distributed diffusion-weighted measurements and 1 *b* = 0 image, with two repetitions. Hence, for the rest of the paper, the first repetition is called *Acquisition 1 (acq1)*, the second *Acquisition 2 (acq2)* and the average of the two *Average (ave)*. The spatial resolution for all three datasets is 3 mm × 3 mm × 3 mm and 3 slices were acquired. Specific parameters are as follows: field of view 19.2 cm, matrix size 64 × 64, read bandwidth 1775 Hz/pixel, partial Fourier factor of 6/8, GRAPPA factor of 2, TR = 5 s, TE = 77/94/102 ms respectively for each *b*-value, and SNR of DWI was estimated to be 9.1/2.6/1.1 respectively (Fillard et al., 2011). The *b* = 0 image has SNR of approximately 15.8.

Local reconstruction techniques. There are several diffusion tensor estimations included in the Tractometer. Diffusion tensors were estimated using our *in-house* log-Euclidean implementation (Arsigny et al., 2006), the *TrackVis* implementation and the *MRtrix* implementation. Moreover, most existing local reconstruction techniques based on the spherical harmonics (SH) representation are currently implemented in the Tractometer. It is beyond the scope of this paper to present the mathematical details of all of these techniques. The reader is referred to the following reviews (Descoteaux, 2008; Seunarine and Alexander, 2009).

SH-based techniques included in the Tractometer are: the diffusion orientation distribution function (ODF) from the numerical Funk-Radon transform (Tuch, 2004) implementation of *TrackVis* (num-ODF), as well as the analytical q-ball imaging solution of (Descoteaux et al., 2007) (a-ODF) and normalized version with constant solid angle (csa) of (Aganj et al., 2010; Tristán-Vega and Aja-Fernández, 2010) (csa-ODF). a-ODF and csa-ODF are implemented



Fig. 3. Invalid Connections (IC) between 2 ROIs of gray matter on the FiberCup and the real data analogies.



Fig. 4. No connections (NC) due to many collisions with the tracking mask or angular constraints not met, both causing the tracking process to finish prematurely on the FiberCup and the real data analogies.

for two SH orders (4 and 6) and all use a Laplace–Beltrami regularization with $\lambda = 0.006$. For the rest of the paper, *r4*, *r6* and *r8* represent maximum SH order 4, 6, and 8 respectively (Descoteaux et al., 2006).

Moreover, spherical deconvolution (SD) techniques were tested at order 6 and 8. We currently have two implementations in the Tractometer: our *in-house* implementation of (Descoteaux et al., 2009), based on diffusion ODF deconvolution to recover the fiber ODF (fODF), and the *MRtrix* implementation of (Tournier et al., 2007), based on the raw diffusion signal deconvolution to recover the fiber orientation transform (FOD). For both SD techniques, default parameters of the constrained regularization were used (Tournier et al., 2012), and the single fiber response function was estimated using voxels with FA value above 0.2 in the white matter mask seen in Fig. 7. Voxels with FA values above 0.2 are only present in the 'U' bundle 4 and the bottom part of bundle 2. A subset of these local estimations are illustrated in Fig. 6. *Tractography: seeding* There are two seeding parameters in the Tractometer. First, whether or not we seed in the whole white matter (WM) or seed from regions of interest (ROI) corresponding to the gray/white interface (as seen in Fig. 7). These masks were manually drawn and are provided in the *Data* section of the Tractometer website (*tractometer.org/data*). Note that gray/white interface ROIs all have the same number of voxels in them (exactly 24 voxels).

At the voxel level, there are also different seeding strategies.

• Our *in-house* strategy randomly draws *N* seeds in the voxel and ensures that all ODF maxima are used (illustrated in Fig. 8). This is to ensure that streamlines will be launched in all principal directions when there is an underlying crossing configuration. Hence, seeds are randomly placed spatially within the voxel, and the tracking direction is a random pick on the maxima of the interpolated ODF at that spatial point.



Fig. 5. Diffusion-weighted images available from different acquisitions of the FiberCup. Here, gradient direction (0, -1, 0), corresponding to the second DWI, is shown for the different *b*-values and acquisitions.

In the case of our *in-house* deterministic and probabilistic tractography algorithms (Girard and Descoteaux, 2012), seeds are also randomly placed in the voxel, but the first tracking direction is always picked according to the fODF distribution, as done by probabilistic tracking.

- The tractography pipelines using *TrackVis* also use multiseeding, which is available with the *-rseed* option.
- *MRtrix* also randomly distributes seeds in voxels but follows a different philosophy. The user can provide a required number of streamlines, *N*, and *MRtrix* will do everything to reconstruct *N* streamlines by randomly putting seeds in the seeding mask provided. Hence, even if a user wants *M* seeds per voxel, *MRtrix* cannot guarantee that exactly *M* seeds will be used in each voxel. It can only approximately get *M* seeds per voxel if the user provides a desired number of streamlines *N* = *VM*, where *V* is the number of voxels in the seeding mask.

Tractography: masking. In the current version of the Tractometer, complete white matter masking is used, using the mask shown in Fig. 7, which was manually segmented. Hence, the tractography process is always stopped when stepping outside this binary tracking mask.

Tractography: angular constraint, radius of curvature and step size. During the tractography procedure, discrete steps (*s* in Fig. 9) are taken to estimate streamlines through the white matter. This step varies from one publication to the other (Tournier et al., 2012; Tournier et al., 2011; Röttger et al., 2011; Hagmann et al., 2003; Parker et al., 2003; Descoteaux et al., 2009; Garyfallidis, 2012; Lazar et al., 2003), and some algorithms have no step size (Mori et al., 1999). Too large of a step has the risk of stepping outside a bundle and into another one. Too small of a step size enhances the risk of deviating from the tract trajectory and increases computational burden. In the current Tractometer, we vary step size with the following four increments: 0.3 mm, 0.6 mm, 1.0 mm and 3.0 mm.

Moreover, depending on the tractography implementation, there is often a maximum allowed angle of curvature between two consecutive directions defined by the maximum aperture angle (θ in Fig. 9), or the radius of curvature (R in Fig. 9). In the current Tractometer, we vary R in the same four increments as the step size. The mathematical relation between R, s, and θ is: $\theta = \min(2 \arcsin(s/(2R)), 90) \in [0, 90^{\circ}]$ (Tournier et al., 2012), which results in constraints shown in Table 1.

Finally, we do not impose a maximum or minimum length for streamlines to perform a fair comparison between methods.

Tractography: deterministic and probabilistic. For HARDI local reconstruction techniques, we use the deterministic streamline implementations of *TrackVis* (*odf_tracker* command), *MRtrix* (*streamtrack SD_STREAM*) (Tournier et al., 2012) and two *in-house*



ave fODF-r6

ave FOD-r6

Fig. 6. Different local estimation methods provided in the Tractometer for *b* = 1500 s/mm² of the average (ave) acquisition in a ROI shown in Fig. 5.



Complete WM seeding

ROI seedings

Complete WM mask

Gray/white matter interface example

Fig. 7. Different seeding strategies for tractography. Complete white matter versus gray-white matter interface seeding, mimicked by ROIs placed at the end of each bundle. Note that each of these ROIs have the same number of voxels.

implementations. The first (*Det. in-house 1* in the tables) follows the local model maxima closest to its incoming direction (Descoteaux et al., 2009). The second technique always follows the direction associated to the maximum value on the sphere within the aperture angle permitted. Moreover, we use the probabilistic streamline implementations of *MRtrix* (*streamtrack SD_PROB*) (Tournier et al., 2012) and our *in-house* implementation (Girard and Descoteaux, 2012; Girard et al., 2012). For DTI, tensorline (Weinstein et al., 1999), FACT (Mori et al., 1999) and Runge–Kutta (rk) (Basser et al., 2000) implementations of *TrackVis* (*dti_tracker* commands) were tested as well as our *in-house* implementation of the tensor advection (TEND) algorithm (Lazar et al., 2003).

Resulting tractography pipelines. The combinatorial number of possible tractograms quickly explodes if we start modifying all



Fig. 8. Multiple seeding scenarios in a crossing configuration. Our *in-house* seeding technique insures that all peaks of a multiple maxima angular profile are covered by the seeding.

possible parameters. Overall, we have N = 57,096 different tractography pipelines. Table 2 illustrates the different steps of the tractography pipeline that were combined.

Ranking system, database and website. An automated system is used to create the pipelines (using the different parameters values combination) to launch all the computations needed to obtain the final streamlines sets. Once the streamlines sets are computed, the system uses the *track_counts* function of *Dipy* (Garyfallidis et al., 2011) to filter those streamlines, using the different sets of ROIs. Each ROIs combination can result in a subset of streamlines that correspond to a specific connection between ROIs. For each of those subsets, the system computes the metrics and updates the database. Once all metrics are computed for all tractography pipelines, each pipeline can be ranked according to its VC, IC, NC, VB, IB and ABC values.

The final results are accessible on the Tractometer website (*tractometer.org*). Users can search, filter and sort the different pipelines according to the different metrics. This way, people will be able to find the best methods and parameters values for their specific needs.

The website also allows users to submit datasets in three categories:

- 1. A modified diffusion-weighted dataset.
- 2. A field of ODFs. The field of ODFs must be submitted as a 3D dataset with discrete spherical function values at every voxel. The discretization of the sphere corresponds to a fifth order tessellation of the icosahedron having 724 points on the hemisphere. This tessellation is dense and has an approximate 4 degrees angle between each sample on the sphere.

Table 1

Tractography angular constraints in degrees. The crossed-out 90 degree angles are crossed-out because they highlight duplicates in the parameters and are thus not generated.

	R			
S	0.3	0.6	1.0	3.0
0.3	60	29	17.3	5.7
0.6	90	60	34.9	11.5
1.0	90 -	90	60	19.2
3.0	90 -	90 -	90	60

3. A dataset of streamlines. The Tractometer currently supports the .trk (*TrackVis*), .tck (*MRtrix*), .bundledata (*brainvisa.info*), and fib (binary and ASCII VTK) streamlines formats.

Hence, a user working on artefact correction or denoising techniques can submit in category (1), a user working on local reconstruction techniques can submit in category (2), or one can submit the streamlines resulting from a new tractography algorithm in category (3). The user must also include a short description of the methods and algorithms used for the creation of this dataset, in order to compare it against what others have proposed. In the case of a diffusion dataset or a field of ODFs submission, our framework will automatically generate the streamlines resulting from this new dataset combined with the tractography pipelines already implemented in the system. Doing so, it will show the impact of new contributions on the final tractography results. As the website grows, more features will be added like new algorithms, the possibility to submit third party libraries, new geometrical metrics and other phantoms, to name a few.



Fig. 9. Deterministic (left) and probabilistic (right) tractography illustrated with angular constraint (θ), radius of curvature (R) (the curvature is 1/R) and step size (s), over fODF glyphs. The mathematical relation between R, s, and θ is: $\theta = \min(2 \arcsin(s/(2R)), 90) \in [0, 90^\circ]$ (Tournier et al., 2012). Deterministic tracking picks the principal direction of the fODF closest to its incoming direction whereas probabilistic streamline tracking randomly picks according to the fODF distribution.

Tabl	е	2
	-	-

List of different tractography options represented in the Tractometer database. 3 acquisitions (Acq.), 11 local reconstruction techniques (Local tech.), 2 seeding strategies, 4 multiseeding numbers (Multiseed), 4 radius of curvature (R), 4 angular constraints (θ), 4 step sizes (s) and 6 different tractography algorithms.

Acq.	<i>b</i> (s/mm ²)	Local tech.	Seeding	Multiseed	R	S	Tracking
acq1 acq2 ave	650 1500 2000	DTI num-ODF-r4,r6 a-ODF-r4,r6 csa-ODF-r4,r6 fODF-r6,r8 FOD-r6,r8	ROI WM	1 9 17 33	0.3 0.6 1.0 3.0	0.3 0.6 1.0 3.0	Det. TractVis Det. MRtrix Prob. MRtrix Det. in-house 1 Det. in-house 2 Prob. in-house

3. Results

Here is an overview of different results and messages that come out of the new analysis of the N = 57,096 tractography streamline outputs in the database. We advise the reader to have Fig. 1 with the ground truth bundle's ID number nearby while reading this section as well as the new definitions of VC (valid connections), IC (invalid connections), NC (no connections), VB (valid bundles), IB (invalid bundles) and ABC (average bundle coverage) in mind. There are many ways to query the database and many possible views and messages that one can extract from it. Here, we decide to start from a very general to a very specific view.

A good tractography pipeline should have a high VC percentage, a high ABC percentage and 7/7 VB found. Table 3 gives a general and per bundle view comparing the success rates of the DTI, HARDI deterministic (HARDI-Det) and HARDI probabilistic (HARDI-Prob) tractography pipelines. Note that out of the 57,096 different pipelines, 7550 pipelines do not recover at least one VC (i.e. 49,546 pipelines have at least 1 VC). For the rest of the tables, we choose to remove these pipelines from statistics because they arise from an aberrant combination of parameters selection in the tractography process. We exclude them to focus on results and messages arising from successful tractography pipelines. Moreover, from Table 3, we note that not all methods are able to retrieve all the 7 out of 7 (7/7) VB. A total of 6,360 out of 57,096 pipelines recover 7/7 VB. This is encouraging and means there is a large number of different parameters options that produce good streamlines outputs which find the 7 VB. In fact, 15%, 13% and 1% of HARDI-Det, HARDI-Prob and DTI pipelines that have at least one VC, also find 7/7 VB. For DTI, it is already a surprise that 58 out of 5065 pipelines recover 7/7 VB, given the difficulty of the fiber crossing configurations of the FiberCup. Most of these 58 DTI pipelines (56/58) come from the TrackVis implementation of the tensorline algorithm (none of the MRtrix and in-house DTI tracking implementations recover 7/7 VB).

In terms of per bundle statistics, we also note from Table 3 that results for DTI and HARDI-Det pipelines show similar results. One must keep in mind that these statistics are computed using pipelines with at least 1 VC, meaning that HARDI-Det statistics are normalized by a much higher pipeline count (PC). The pipelines from the HARDI-Prob family show, on average, a lower bundle recovery rate and a higher ABC. The standard deviation on ABC for DTI, HARDI-Det and HARDI-Prob pipelines is in the interval [13.1%, 20.6%], [14.7%, 19.2%] and [23.9%, 29.1%], respectively. Even with this high standard deviation, the results show that probabilistic pipelines are better at recovering the full fiber bundles. The standard deviation table corresponding to Table 3 is provided in the supplementary materials. For the rest of the results, we choose to compute statistics only on tractography pipelines with 7/7 VB.

Acquisition. Table 4 shows the effect of the different acquisition options on the tractography results. We first note that connectivity metrics are improved when using the averaged acquisition. We also see that acq1 is systematically better than acq2. Best scores

are always obtained with *b*-value 1500 s/mm². Moreover, given its low SNR, it is not surprising that the *b*-value 2000 s/mm² has the worst connectivity scores. Also, as expected, b-value 650 s/ mm² has a much lower count of 7/7 VB. It has a high SNR, but the local angular profiles reconstructed from it do not properly recover crossing configurations, even with HARDI techniques. However, the averaged *b*-value 650 s/mm² acquisition also results in the best ABC. This is surely due to the over-smoothed local angular ODF profiles that are reconstructed. Finally, note that in the best case, we only have 12.7% valid connections. This is quite low and reflects the aggressiveness of the stopping criteria in the tractography pipelines. Based on Table 4, we compute the rest of the statistics only using the averaged acquisition and *b*-value 1500 s/mm². By doing this, we gradually zoom into the best tractography pipelines. The standard deviation table corresponding to Table 4 is provided in the supplementary materials.

Local reconstruction techniques. Table 5 shows the effect of the different local reconstruction techniques. Sharp angular distributions have more success at recovering 7/7 VB (highest count), starting with FODs from MRtrix, followed by our in-house fODFs and the smoother csa-ODF, a-ODF and num-ODF reconstruction techniques. Again, in terms of connectivity metrics, sharp angular profiles (FODs and fODFs) show the highest VC and lowest IC and IB. However, this is at the price of having more NC. DTI has an IB count of 25. HARDI-Det has an IB count of approximately 17.5 for smooth profiles (num-ODF, a-ODF and csa-ODF) and approximately 12.5 for sharper profiles (FOD, fODF). This is approximately 5 IB less for the sharper angular profiles, which is considerable. Moreover, HARDI-Prob has an IB count of approximately 22 for sharp models, which is also considerable. Also note that no probabilistic pipeline successfully recovered 7/7 VB for the smoother ODF profiles. Finally, as expected, fODFs/FOD combined with probabilistic tracking have the best ABC. At this point, we set the local reconstruction techniques to FOD-r6,r8 and fODF-r6,r8 for the rest of the analysis. There was no significant difference between maximal SH order 4, 6, and 8 reconstructions (shown Table 4 of the supplementary materials).

Tractography parameters: step size, curvature, seeding. Considering tractography pipelines that recover 7/7 VB with the averaged acquisition at *b*-value 1500 s/mm² and the FOD-r6,r8 or fODFr6,r8, we do not find a trend for best combination of step size, curvature and seeding strategy to obtain high VC, low IB and high ABC. The step size, the curvature and the seeding strategy seem to be very dependent on the choice of the tractography algorithm. Hence, averaging results from many different tractography pipelines does not provide any interesting observation or recommendation (shown in Tables 5 and 6 of the supplementary materials for completeness). Overall, higher ABC is generally obtained with a seeding strategy using more than 1 seed, but is similar for all multiseeding tested (9, 17, and 33). VC is also generally slightly higher on average using a single seed. Finally, in general, the number of IB is lower when ROI seeding and a single seed is used.

Best of. We finish by reporting an overview of best of tractography pipelines sorted in terms of maximum VC, minimum IB with

Table 3

General view of the statistics of DTI, HARDI deterministic and HARDI probabilistic tractography pipelines. Best ABC and PC % are for bundles 4 and 6. Bundle 3 is badly covered but recovered with high frequency. Bundles 2 and 3 are harder to recover. HARDI-Prob pipelines produce highest ABC. The corresponding table of standard deviation is provided in table 1 of the supplementary materials.

Pipeline	Pipeline Pipeline Count (PC)			Bundle 1	Bundle number						
	Total	VC > 0	7/7 VB	1	2	3	4	5	6	7	
DTI	5616	5065	58	72.8 36.2	19.6 21.4	52.0 30.4	89.9 66.0	72.3 34.0	93.4 51.8	57.3 29.2	PC (%) ABC (%)
HARDI-Det.	34,632	33,082	5260	70.2 42.2	38.3 31.9	38.6 27.5	99.7 67.4	61.3 35.2	80.7 53.8	60.0 33.0	PC (%) ABC (%)
HARDI-Prob.	16,848	11,399	1042	44.4 46.0	22.2 38.0	24.4 37.2	90.1 63.9	53.1 43.4	50.7 51.7	29.3 40.9	PC (%) ABC (%)
Total	57,096	49,546	6360	64.5 42.1	32.7 32.2	36.7 29.4	96.5 66.5	60.5 36.6	75.1 53.3	52.6 33.6	PC (%) ABC (%)

Table 4

Table of the different acquisition options. The averaged *b*-value 1500 s/mm² acquisition shows the best scores with highest VC, lowest NC and IC and thus, best ratios. The corresponding table of standard deviation is provided in the supplementary materials.

Acq.	<i>b</i> (s/mm ²)	$\frac{VC}{VC+IC}$ (%)	VC (%)	IC (%)	NC (%)	IB (%)	ABC (%)	Count(/6360)
acq1	650	48.8	3.5	3.8	92.7	25.3	57.4	73
acq1	1500	63.8	9.5	5.5	85.1	19.1	54.1	840
acq1	2000	59.8	6.7	4.8	88.5	20.2	50.6	605
acq2	650	42.3	1.1	1.3	97.7	21.8	56.4	24
acq2	1500	60.3	8.8	6.5	84.7	17.3	51.1	1103
acq2	2000	60.8	6.6	4.6	88.8	17.9	49.5	931
ave	650	47.4	4.1	4.7	91.1	24.8	58.4	70
ave	1500	70.2	12.7	6.4	80.9	15.7	54.6	1658
ave	2000	63.7	8.4	5.4	86.3	17.8	52.7	1056

Table 5

Table of HARDI local reconstruction techniques. Sharp angular distributions have more success at recovering 7/7 VB. The corresponding standard deviation table is provided in the supplementary materials.

Tracking	Local tech.	$\frac{VC}{VC+IC}$ (%)	VC (%)	IC (%)	NC (%)	IB (%)	ABC (%)	Count(/1658)
det	DTI	27.5	7.3	19.4	73.3	25.0	52.3	10
det	num-ODF	56.4	11.5	9.9	78.7	17.9	51.8	149
det	a-ODF	58.5	14.7	10.7	74.6	17.5	53.7	205
det	csa-ODF	58.7	14.8	10.7	74.4	16.9	52.4	215
det	fODF	89.1	9.2	1.4	89.4	12.7	53.2	367
det	FOD	77.9	16.6	5.5	77.9	12.2	52.6	499
prob	fODF	57.4	1.6	0.8	97.6	19.2	57.0	29
prob	FOD	53.4	7.3	6.2	86.5	24.9	68.1	184

maximum VC, minimum NC and maximum ABC. As seen in Table 6, we report the best of each family of tractography pipelines and indicate their corresponding connectivity metrics and rank. The line corresponding to the overall best tractography pipeline is always indicated with a gray background and the resulting valid connection streamlines are also illustrated in Fig. 10. For comparison, we also illustrate VC of several *worst* tractography pipelines in Fig. 10.

- 1. In terms of maximum VC, the best deterministic tractography pipeline recovers nearly 25% VC, the best probabilistic pipeline 15% and the best DTI pipeline 10%. In general, the best of deterministic pipelines have much higher VC percentages than probabilistic pipelines. When looking at the top 100 pipelines, most combinations of step size, curvature and seeding strategy appear. The ave-b1500 dataset is the only one used in the top 100 pipelines and the FOD-r6,r8 are the most common local techniques. Note that the csa-ODF-r4,r6 come up only once in the top 100 pipelines. Finally, we note that the overall best pipeline in terms of maximum VC is the *in-house 2* tractography algorithm, with the ave-b1500, FOD-r8 from *MRtrix*, a full white matter seeding with 1 seed per voxel, step size of 1 mm and radius of curvature of 3 mm.
- 2. In terms of minimum IB and maximum VC, the best pipeline produces 15.6% of VC, whereas the VC decreases by 4.7% for the pipeline coming at the second rank. The best pipeline is from our *in-house 1* tractography algorithm, with ave-b1500 dataset, FOD-r6 from MRtrix, seeding only from ROIs with 1 seed per voxel, a step size of 0.3 mm and radius of curvature 0.6 mm. We also note that the top 8 pipelines produce 0 IB! With the exception of the best pipeline that has 83.6% of NC, all other pipelines in the top 100 have NC in the interval [89%, 99.6%]. Moreover, the best pipeline has the highest VC but has one of the worst ABC. Overall, in the top 100 pipelines, the ave-b1500 dataset appears most often, the local reconstruction techniques are mainly the FOD-r6,r8 and the fODF-r6,r8, the most common step size is 0.3 mm, the curvature is always greater or equal to 0.6 mm, and all combinations of seeding and multiseeding strategies appear in the top 100.
- 3. In terms of minimum NC, the best pipeline produces 60.4% of NC and comes from the deterministic *MRtrix* tractography algorithm with the ave-b1500 dataset, our *in-house* csa-ODF-r4 profiles, seeding only from ROIs with 1 seed per voxel, a step size of 3 mm and radius of curvature 1 mm. We also note a wide range of ratio VC/(VC + IC), which is in the interval [36.6%, 78.8%] in the top 100 pipelines. All HARDI local techniques appear in

Table 6

Summary of pipelines recovering 7/7 VB from the database, without other filtering. Pipelines are sorted by maximum VC, minimum IB and maximum VC, minimum NC and maximum ABC.

Tracking Acq. b local t	ech. Seeding/	s/R	VC	VC	IC	NC	IB	ABC	Rank
(s/mm ²)	Multiseed	(mm)	VC+IC	(%)	(%)	(%)	(/39)	(%)	(/6,360)
Best of : maximum VC									
Det. in-house 1 ave 1500 FOD-	r6 ROI/1	1.0/0.6	72.8	23.3	8.7	68.1	11	38.2	6
Det. in-house 2 ave 1500 FOD-	r8 WM/1	1.0/3.0	78.8	24.7	6.6	68.6	14	54.8	1
Det. MRtrix ave 1500 csa-O	DF-r6 ROI/1	3.0/3.0	64.2	21.2	11.8	67.0	8	28.7	71
Det. TrackVis ave 1500 num-C	DDF ROI/33	0.3/0.3	74.8	12.1	4.1	83.9	16	53.8	1673
Prob. in-house ave 1500 FOD-	r8 ROI/9	0.3/0.6	59.9	14.6	9.8	75.7	19	57.3	995
Prob. MRtrix. ave 1500 FOD-	r8 ROI/9	0.3/0.6	58.5	11.8	8.4	79.8	20	56.6	1749
Det. TrackVis-rk2 acq1 1500 DTI	WM/17	3.0/1.0	45.2	10.0	12.1	77.8	21	46.8	2450
Best of : mininum IB and maximum VC									·
Det. in-house 1 ave 1500 FOD-	r6 ROI/1	0.3/0.6	95.7	15.6	0.7	83.7	0	29.8	1
Det. in-house 2 ave 1500 FOD-	r8 ROI/1	0.3/3.0	79.7	20.5	5.2	81.9	4	34.3	178
Det. MRtrix ave 1500 FOD-	r6 ROI/9	0.6/3.0	99.3	10.9	0.1	89.0	0	42.5	2
Det. TrackVis ave 1500 num-C	DDF WM/9	0.6/1.0	87.8	5.8	0.8	93.4	4	41.9	231
Prob. in-house acq2 1500 FOD-	r8 ROI/1	1.0/3.0	71.0	7.6	3.1	89.2	7	26.8	442
Prob. MRtrix. acq2 2000 FOD-	r8 ROI/9	0.6/3.0	67.6	1.0	0.5	98.5	6	28.5	408
Det. TrackVis-tl ave 2000 DTI	WM/33	0.3/0.3	30.0	5.7	13.4	80.9	17	48.0	2991
Best of : mininum NC									
Det. in-house 1 ave 1500 FOD-	r6 ROI/1	3.0/1.0	60.6	20.8	13.5	65.6	12	31.7	38
Det. in-house 2 ave 1500 FOD-	r6 ROI/33	3.0/3.0	44.4	16.2	20.2	63.6	18	47.1	16
Det. MRtrix ave 1500 csa-O	DF-r4 ROI/1	3.0/1.0	53.5	21.2	18.4	60.4	11	28.5	1
Det. TrackVis ave 1500 num-C	DDF WM/1	1.0/0.6	51.5	10.7	10.1	79.2	23	51.3	1460
Prob. in-house ave 1500 FOD-	r8 ROI/9	0.3/0.6	59.9	14.6	9.8	75.7	19	57.3	797
Prob. MRtrix. ave 1500 FOD-	r8 ROI/17	0.3/0.6	54.8	11.4	9.4	79.2	20	64.9	1459
Det. TrackVis-tl ave 1500 DTI	WM/33	0.3/0.3	24.6	7.5	23.1	69.4	24	52.9	131
Best of : maximum ABC									
Det. in-house 1 ave 1500 fODF	-r6 WM/33	3.0/1.0	89.9	9.5	1.1	89.4	24	75.0	315
Det. in-house 2 ave 1500 csa-O	DF-r4 WM/33	0.3/3.0	56.7	11.2	8.5	80.3	30	80.9	120
Det. MRtrix ave 1500 FOD-	r8 WM/33	3.0/1.0	73.1	17.0	6.2	76.7	26	73.6	370
Det. TrackVis ave 1500 num-0	DDF ROI/33	1.0/0.6	51.5	10.1	9.4	80.5	35	73.6	368
Prob. in-house ave 1500 FOD-	r8 WM/33	1.0/3.0	67.2	6.7	3.3	90.1	31	91.8	1
Prob. MRtrix. ave 1500 FOD-	r6 WM/33	0.3/1.0	52.8	5.0	4.4	90.6	31	90.3	3
Det. TrackVis-tl acq1 1500 DTI	WM/33	3.0/3.0	33.7	6.1	12.0	81.9	26	61.4	1330
Worst of : maximum TC			•			•	•		
Det. in-house 1 ave 2000 num-0	DDF WM/33	0.3/1.0	96.7	0.7	0.0	99.4	3	37.6	6291
Prob. MRtrix. acq1 1500 fODF	-r8 WM/33	1.0/3.0	10.5	0.0	0.2	99.8	18	21.4	6360
Det. TrackVis-tl acq1 650 DTI	WM/9	3.0/1.0	18.4	3.4	15.3	81.3	23	40.7	5653

the top 100, including the smoother ones (num-ODF, a-ODF and csa-ODF). Overall, the ave-b1500 is the most appearing dataset, the most common step size is greater or equal to 1 mm, but mainly s = 3 mm, and the radius of curvature is most often $R \ge 1$ mm. Finally, all combinations of seeding and multiseeding strategies appear in the top 100.

4. In terms of maximum ABC, the best ABC percentage is obtained using probabilistic tracking. In fact, the top 100 pipelines are exclusively probabilistic ones. The best pipeline obtains an ABC of 91.8% but, at the same time, has a low VC percentage and the highest number of IB, with 33 invalid bundles! In fact, the IB is always in the interval [23, 32], which is a huge number of invalid bundles. The first deterministic algorithm is ranked 120. We also note that DTI produces poor ABC results. Overall, in the top 100, all local techniques are FOD-r6,r8 and most pipelines use the WM seeding with a multiseeding of 33 seeds per voxel. Finally, in the top 100, acq1, acq2 and ave for *b*-value 1500 s/mm² are equally common, the step size is most often smaller or equal to 1 mm and the radius of curvature is larger or equal to 1 mm.

4. Discussion

It is important to first note that results reported in this paper have changed compared to our MICCAI paper (Côté et al., 2012), which only had 1,152 tractography pipelines. Moreover, in the current version of the Tractometer, we ensure that all ROIs have the same number of voxels. We encourage the community to query the database differently and extract other messages that we might have omitted in this paper.

In general, a conclusion based on techniques available in the database is that the current best tractography pipeline configuration for optimal trade-off between VC, IC, NC, VB, IB and ABC is using the averaged dataset with *b*-value 1500 s/mm², a sharp local estimation from spherical deconvolution and a deterministic tracking algorithm handling fiber crossings such as our *in-house* or *MRtrix* implementations. However, it is not straightforward to have general conclusions for the step size, curvature, seeding strategies. We now discuss each part of the processing pipeline in turn.

4.1. Acquisition

Limitations of the FiberCup dataset. The FiberCup phantom dataset is not perfect. The anisotropy of the phantom is quite low and thus privileges a certain class of techniques based on an angular distribution content of the DWI data. Raw signal modeling-based approaches are disadvantaged (such as implemented in FSL) and not well suited for the FiberCup dataset, as shown in (Fillard et al., 2011). The FiberCup dataset only provides three *b*-value acquisitions, with the *b*-value 2000 s/mm² too noisy to be useful



(a) Maximum VCAcq./b:ave/1500Local tech.:FOD-r8Tracking:Det. in-house 2s/R - Seed: $1.0/3.0 \cdot WM/1$ VC/Nb. Seeds:507/2051





(c) Minimum NCAcq./b:ave/1500Local tech.:csa-ODF-r4Tracking:Det. MRtrixs/R - Seed:3.0/1.0 - ROI/1VC/Nb. Seeds:61/288



 (d) Maximum ABC

 Acq./b:
 ave/1500

 Local tech.:
 FOD-r8

 Tracking:
 Prob. in-house

 s/R - Seed:
 1.0/3.0 - WM/33

 VC/Nb. Seeds:
 4527/67,683



 (e) Maximum
 ABC, DTI-Det.

 Acq./b:
 ave/1500

 Local tech.:
 DTI

 Tracking:
 Det. TrackVis-tl

 s/R - Seed:
 3.0/3.0 - WM/33

 VC/Nb. Seeds:
 3816/67.683

(t) Minimum VC, DTI-Det.Acq./b:acq1/650Local tech.:DTITracking:Det. TrackVis-tls/R - Seed:3.0/1.0 - WM/9VC/Nb. Seeds:589/18,459

 (g) Minimum VC, HARDI-Det.

 Acq./b:
 acq1/1500

 Local tech.:
 fODF-r8

 Tracking:
 Prob. MRtrix

 s/R - Seed:
 1.0/3.0 - WM/33

 VC/Nb. Seeds:
 383/67.683

 (h) Minimum VC, Hardi-Prob.

 Acq./b:
 ave/2000

 Local tech.:
 num-ODF

 Tracking:
 Det. in-house 1

 s/R - Seed:
 0.3/1.0 - WM/33

 VC/Nb. Seeds:
 17/67,683



and the *b*-value 650 s/mm² resulting in over-smoothed local ODF profiles challenged in the crossing configurations. It is important to have richer *b*-value phantoms in a pursuit of having an optimal *b*-value acquisition for HARDI tractography.

Moreover, the FiberCup phantom does not provide a real 3D space example and is limited to the 2D plane. Other phantoms should take into account more complex bundles. Or, ideally, new techniques should be developed to compare streamlines bundles within a brain, as attempted in (Baumgartner et al., 2012). Of course, one has to be careful not to develop or tune his tractography algorithm to best perform solely on the FiberCup dataset. Since our preliminary version of this paper (Côté et al., 2012), several groups have contacted us to add new phantom datasets, such as Fieremans et al., 2008 (url: *www.nitrc.org/projects/diffusion-data*), to the Tractometer. We are currently investigating these new phantoms.

Averaging. It is reassuring and expected (Table 4) that averaging the two repetitions (acq1 and acq2) helps improve the connectivity metrics. However, the reader must keep in mind that this doubles the acquisition time, which is often not possible in clinical applications. This motivates the development of state-of-the-art denoising and noise correction techniques (Descoteaux et al., 2008; Coupé et al., 2010; Aja-Fernández et al., 2011; Brion et al., 2012). We are also currently considering providing masks and ROIs in a upsampled 128x128x6 space, so that groups developing new super-resolution techniques (Nedjati-Gilani et al., 2008; Scherrer et al., 2012) or using upsampling (Dyrby et al., 2011; Raffelt et al., 2012; Smith et al., 2012a) can use the Tractometer to evaluate their techniques. Direction undersampling. Finally, groups working on novel compressed sensing and undersampling acquisitions with limited number of gradient directions can use the Tractometer to compare their novel techniques. The diffusion community needs a HARDI reconstruction acquisition scheme that is similar to a DTI-like scheme. Hence, it is important to seek high quality fiber crossing tractography results obtained from DTI-like acquisitions (approximately 12–30 directions).

4.2. Local estimation techniques

First, sharp angular distributions (FODs and fODFs) had more success than smoother ODFs (num-ODF, a-ODF, csa-ODF). Hence, in general, spherical deconvolution performed better than numerical and analytical ODFs. Depending on the acquisition used and its noise level, direct effects of local estimation techniques could also be seen in the resulting streamlines. Therefore, as the Tractometer grows, it can serve to further explore the effect of SH maximum order, λ -regularization parameters, response function estimation for deconvolution, amongst others. Finally, some SH-based techniques have not been implemented, such as spherical ridgelets (Michailovich and Rathi, 2009), spherical wavelets (Kezele et al., 2010), and the diffusion orientation transform (DOT) (Özarslan et al., 2006), but should soon appear in the Tractometer as we include more libraries, such as Dipy (Garyfallidis et al., 2011) and Camino (Cook et al., 2006). Similarly, we would like to compare multi-compartment parametric models like ball & sticks (Behrens et al., 2007) or multi-tensor (Kreher et al., 2005).

4.3. Tractography parameters

Step size. In the current literature, a general rule of thumb for choosing the step size is to set the step size as half the spatial acquisition grid, although (Tournier et al., 2012) recently suggested 1/10 the spatial acquisition grid. Note that some tractography techniques do not require any explicit step size, such as FACT (Mori et al., 1999) implemented in *DTI studio (www.dtistudio.org)*, which steps according to the voxel size, and should be considered in future comparisons. The Tractometer has a large number of pipelines that produce 7/7 VB with good valid/invalid connection trade-off and acceptable average bundle coverage, using all possible step sizes tested. The step size clearly depends on other parameters and the implementation of the tractography algorithm as such. Optimal step size selection remains an open question.

Interpolation. In the current tractography techniques provided in the Tractometer, interpolation techniques have not been thoroughly studied. During the fiber tracking process, one wants to combine local neighborhood information. For this purpose, interpolation is used. Runge–Kutta interpolation is available in *TrackVis* when using the tensor model, but most other tractography techniques implemented use tri-linear interpolation on the field of ODFs. Should this interpolation take place on the original DWI data, on the field of DTs/ODFs, or simply on the principal directions extracted? When done on the field of principal directions, voxels at the boundary of the tracking mask are often problematic, and it is thus commonly performed on the field of DT/ODFs. However, interpolation certainly remains an open question and can considerably increase computation time of tractography pipelines. It also needs to be further addressed in the future.

Masking. Defining a good tracking mask is crucial for tractography algorithms (Guevara et al., 2011; Girard and Descoteaux, 2012). The novice tractography user soon realizes that if tracking is done on the whole brain, tracts can be found (i) passing through the ventricles; (ii) in between left and right hemispheres, through the inter-hemispheric space; and (iii) in between cortical regions, through sulci, among other physically impossible regions. Often, a classical approach is to define the mask using a thresholded fractional anisotropy (FA) map, often thresholded at values between 0.1 and 0.2. FA is fundamentally flawed in crossing and curving voxels and thus produces masks containing holes. In the Tractometer, the complete mask shown in Fig. 7 is used. We found that this is an aggressive stopping criteria (Girard and Descoteaux, 2012), leading to a large number of NC (more than 60% of streamlines), as seen in Fig. 4, in most tractography algorithms. Recent stateof-the-art techniques take into account information about the anatomy (Iturria-Medina et al., 2008; Girard and Descoteaux, 2012; Girard et al., 2012; Bloy et al., 2012; Smith et al., 2012a; Smith et al., 2012b) to improve the behavior of tractography. These techniques stress the importance for tractography algorithms not to stop in cerebral spinal fluid (CSF), not to stop in the white matter and terminate in gray matter or out of the brainstem (Girard and Descoteaux, 2012; Smith et al., 2012a). Finding the optimal boundary and masking conditions for tractography algorithms remains an open question.

Seeding. In general, using both complete and ROI seeding, 1 seed per voxel produces the best trade-off between valid and invalid connections. However, using only 1 seed per voxel suffers from a low ABC. The more seeds per voxel, the more IC but the better the ABC. In the end, the best ABC is obtained from complete seeding and 33 seeds per voxel but at the price of having more than 24 invalid bundles, which is a huge problem. Hence, the Tractometer currently suggests that both ROI and complete seeding are appropriate seeding strategies and should be used with care to control the proportion of valid/invalid connections. Complete fiber tractography (from all white matter voxels) should probably be done with a low seeding number per voxel to avoid invalid connections as much as possible. On the other hand, if extra information (anatomical, functional, amongst others) is available and can be used to filter out invalid connections, a large number of seeds per voxel can be used to obtain a good average bundle coverage.

Seeding and masking certainly have a huge impact on the fiber count and the density of fiber bundles. In a sense, "easier" bundles such as bundles 4 and 6 (those that have less fiber crossing configurations along their path), end up artificially over-estimated, as reported in (Smith et al., 2012b), with a much larger number of streamlines, compared to more "difficult" bundles such as bundles 2 and 3. Hence, as mentioned in (Jones et al., 2013), fiber count should be avoided. In (Smith et al., 2012b), it is advised to correct for this fiber density bias using a new filtering approach and by seeding only from the gray/white matter interface. Seeding and masking clearly remain open questions for the tractography community.

4.4. Deterministic and probabilistic tractography

Fiber tracking is an intuitive process, but one with many underlying parameters mentioned in the previous paragraphs. Streamlines are recovered by propagating through a field of DTs, ODFs, fODFs, FODs, or any other pre-computed set of directions. What directions to follow? How to follow them? How to numerically extract them? These questions are crucial in tractography and remain open. Many families of algorithms exist, just to name a few: deterministic, probabilistic, geodesic, and global algorithms. We are pursuing an extension for connectivity matrices provided by other probabilistic, geodesic (Péchaud et al., 2009; Sepasian et al., 2009), global tractography algorithms (Jbabdi et al., 2007; Kreher et al., 2008; Fillard et al., 2009; Reisert et al., 2011) or any other fiber tracking approach.

The Tractometer is currently developed for streamline-based deterministic and probabilistic algorithms. Deterministic techniques have a lower ABC percentage than probabilistic ones, but have a much better valid/invalid connection trade-off. Probabilistic tractography techniques are surely disadvantaged by the limitations of the FiberCup datasets but in any case, they are, in nature, much more aggressive in the way they randomly explore tracking directions from the field of fiber ODFs provided to the fiber tracking algorithm. Hence, probabilistic pipelines have a tendency to produce a large number of no and invalid connections. As for multiseeding strategies, we believe they should be used with care and only if extra information is available to filter out invalid connections.

5. Conclusion

We have developed the Tractometer, an online system for the evaluation of tractography pipelines. Overall, we have shown that *MRtrix* and our *in-house* tools based on spherical deconvolution currently provide the best rankings in terms of valid/invalid connections. *TrackVis* is based on q-ball ODFs or DTI, and thus, does not perform as well, just as our *in-house* tracking based on q-ball ODFs and DTI. Our *in-house* tracking will be available shortly in *Dipy* (Garyfallidis et al., 2011).

In summary, the most important messages that come out of the Tractometer in its current state are: (i) Averaging improves results. (ii) Sharp angular ODF profiles help the tractography algorithm. (iii) The more you add seeds, the more invalid connections (IC) you get, and one should be careful about randomly seeding a large number of seeds in the complete white matter. (iv) Probabilistic streamline tracking has highest ABC at the price of severely increasing NC and IC. (v) Deterministic streamline techniques

show the best valid/invalid connection trade-off in our connectivity metrics. The (iv)–(v) messages are contrary to the popular belief that probabilistic tractography gives, in general, better results than deterministic tractography. We have shown that this is not the case when using the FiberCup phantom. Hence, probabilistic tractography algorithms should be used with care, especially in global connectomics studies.

Of course, these are only the first steps of the Tractometer, but we believe that, as the community contributes to the system with more, and better phantoms, this new system can have a positive impact on the dMRI community. Just as the machine learning and computer vision communities have used benchmarks to move forward in algorithm design and evaluation, the dMRI community needs to do the same to answer open questions. Only then can new tractography algorithms be compared to the state-of-the-art and their contributions quantified.

Send us your corrected raw diffusion data, your ODFs or your fiber streamlines at *tractometer.org* and you will be compared and ranked against other state-of-the-art techniques!

Acknowledgments

We would like to thank Compute Canada for access to High Performance Computing (HPC) resources and thank NeuroSpin for the public FiberCup dataset (url: *www.lnao.fr/spip.php?rubrique79*).

Appendix A. Supplementary material

Supplementary data associated with this article can be found, in the online version, at http://dx.doi.org/10.1016/j.media.2013. 03.009.

References

- Aganj, I., Lenglet, C., Sapiro, G., Yacoub, E., Ugurbil, K., Harel, N., 2010. Reconstruction of the orientation distribution function in single- and multiple-shell q-ball imaging within constant solid angle. Magnetic Resonance in Medicine 64, 554–556.
- Aja-Fernández, S., Tristán-Vega, A., Hoge, W.S., 2011. Statistical noise analysis in GRAPPA using a parametrized noncentral Chi approximation model. Magnetic Resonance in Medicine 65. 1195–1206.
- Anderson, A.W., Choe, A.S., Stepniewska, I., Colvin, D.C., 2006. Comparison of brain white matter fiber orientation measurements based on diffusion tensor imaging and light microscopy. Proceedings of the IEEE Engineering in Medicine and Biology Society 1, 2249–2251.
- Arsigny, V., Fillard, P., Pennec, X., Ayache, N., 2006. Log-euclidean metrics for fast and simple calculus on diffusion tensors. Magnetic Resonance in Medicine 56, 411–421.
- Bach, M., Stieltjes, B., Fritzsche, K., Semmler, W., Laun, F.B., 2011. A diffusion tensor resolution phantom. In: International Society for Magnetic Resonance in Medicine (ISMRM), Montreal, Canada, p. 3975.
- Basser, P., Pajevic, S., Pierpaoli, C., Duda, J., Aldroubi, A., 2000. In vivo fiber tractography using DT-MRI data. Magnetic Resonance in Medicine 44, 625–632.
- Baumgartner, C., Michailovich, O., Levitt, J., Pasternak, O., Bouix, S., Westin, C.F., Rathi, Y., 2012. A unified tractography framework for comparing diffusion models on clinical scans. In: International Conference on Medical Image Computing and Computer Assisted Intervention (MICCAI'12) – Computational Diffusion MRI, Workshop, pp. 27–32.
- Behrens, T.E.J., Johansen-Berg, H., Jbabdi, S., Rushworth, M.F.S., Woolrich, M.W., 2007. Probabilistic diffusion tractography with multiple fibre orientations: what can we gain? NeuroImage 34, 144–155.Bloy, L., Ingalhalikar, M., Batmanghelich, N.K., Schultz, R.T., Roberts, T.P.L., Verma, R.,
- Bloy, L., Ingalhalikar, M., Batmanghelich, N.K., Schultz, R.T., Roberts, T.P.L., Verma, R., 2012. An integrated framework for high angular resolution diffusion imagingbased investigation of structural connectivity. Brain Connectivity 2, 69–79.
- Brion, V., Riff, O., Descoteaux, M., Mangin, J.F., Bihan, D.L., Poupon, C., Poupon, F., 2012. The parallel Kalman filter: an efficient tool to deal with real-time non central noise correction of hardi data. In: ISBI, IEEE, pp. 34–37.
- Budde, M.D., Frank, J.a., 2012. Examining brain microstructure using structure tensor analysis of histological sections. NeuroImage 63, 1–10.
- Campbell, J.S.W., Savadjiev, P., Siddiqi, K., Pike, G.B., 2006. Validation and regularization in diffusion mri tractography. In: Third IEEE International Symposium on Biomedical Imaging (ISBI): from Nano to Macro, Arlington, Virginia, USA, pp. 351–354.
- Cook, P., Bai, Y., Nedjati-Gilani, S., Seunarine, K., Hall, M., Parker, G., Alexander, D., 2006. Camino: open-source diffusion-mri reconstruction and processing. In:

International Society for Magnetic Resonance in Medicine, Washington, Seatle, USA, p. 2759.

- Côté, M.A., Boré, A., Girard, G., Houde, J.C., Descoteaux, M., 2012. Tractometer: online evaluation system for tractography. In: MICCAI 2012, Part I, LNCS 7510, Nice, France, pp. 698–705.
- Coupé, P., Manjòn, J.V., Gedamu, E., Arnold, D., Robles, M., Collins, D.L., 2010. Robust Rician noise estimation for MR images. Medical Image Analysis 14, 483–493.
- Dauguet, J., Peled, S., Berezovskii, V., Delzescaux, T., Warfield, S.K., Born, R., Westin, C.F., 2007. Comparison of fiber tracts derived from in-vivo dti tractography with 3d histological neural tract tracer reconstruction on a macaque brain. NeuroImage 37, 530–538.
- Descoteaux, M., 2008. High Angular Resolution Diffusion MRI: from Local Estimation to Segmentation and Tractography. Ph.D. thesis, Université de Nice-Sophia Antipolis.
- Descoteaux, M., Angelino, E., Fitzgibbons, S., Deriche, R., 2006. Apparent diffusion coefficients from high angular resolution diffusion imaging: Estimation and applications. Magnetic Resonance in Medicine 56, 395–410.
- Descoteaux, M., Angelino, E., Fitzgibbons, S., Deriche, R., 2007. Regularized, fast, and robust analytical q-ball imaging. Magnetic Resonance in Medicine 58, 497–510.
- Descoteaux, M., Deriche, R., Knösche, T.R., Anwander, A., 2009. Deterministic and probabilistic tractography based on complex fibre orientation distributions. IEEE Transactions in Medical Imaging 28, 269–286.
- Descoteaux, M., Poupon, C., in press. Diffusion-weighted MRI. In: Comprehensive Biomedical Physics, Elsevier.
- Descoteaux, M., Wiest-Daesslé, N., Prima, S., Barillot, C., Deriche, R., 2008. Impact of rician adapted non-local means filtering on hardi. In: Medical Image Computing and Computer-Assisted Intervention (MICCAI), pp. 122–130.
- Dyrby, T.B., Lundell, H.M., Liptrot, M.G., Burke, M.W., Ptito, M., Siebner, H.R., 2011. Interpolation of DWI prior to DTI reconstruction, and its validation. In: International Society for Magnetic Resonance in Medicine, Montreal, Canada, p. 1917.
- Fieremans, E., Deene, Y.D., Delputte, S., zdemir, M.S.O., Achten, E., Lemahieu, I., 2008. The design of anisotropic diffusion phantoms for the validation of diffusion weighted magnetic resonance imaging. Physics in Medicine and Biology 53, 5405–5419.
- Fillard, P., Descoteaux, M., Goh, A., Gouttard, S., Jeurissen, B., Malcolm, J., Ramirez-Manzanares, A., Reisert, M., Sakaie, K., Tensaouti, F., Yo, T., cois Mangin, J.F., Poupon, C., 2011. Quantitative evaluation of 10 tractography algorithms on a realistic diffusion mr phantom. NeuroImage 56, 220–234.
- Fillard, P., Poupon, C., Mangin, J., 2009. A novel global tractography algorithm based on an adaptive spin glass model. In: Proceedings of Medical Image Computing and Computer-Assisted Intervention (MICCAI'09), pp. 927–934.
- Garyfallidis, E., 2012. Toward an accurate brain tractography. Ph.D. thesis, University of Cambridge.
- Garyfallidis, E., Brett, M., Amirbekian, B., Nguyen, C., Yeh, F., Halchenko, Y., Nimmo-Smith, I., 2011. Dipy – a novel software library for diffusion MR and tractography. In: 17th Annual Meeting of the Organization for Human Brain Mapping.
- Girard, G., Chamberland, M., Houde, J.C., Fortin, D., Descoteaux, M., 2012. Neurosurgical tracking at the Sherbrooke Connectivity Imaging Lab (SCIL). In: International Conference on Medical Image Computing and Computer Assisted Intervention (MICCAI'12) – DTI Challenge, Workshop, pp. 55–73.
 Girard, G., Descoteaux, M., 2012. Anatomical tissue probability priors for
- Girard, G., Descoteaux, M., 2012. Anatomical tissue probability priors for tractography. In: International Conference on Medical Image Computing and Computer Assisted Intervention (MICCAI'12) – Computational Diffusion MRI, Workshop, pp. 174–185.
- Guevara, P., Duclap, D., Marrakchi-Kacem, L., Rivière, D., Cointepas, Y., Poupon, C., Mangin, J.F., 2011. Accurate tractography propagation mask using t1-weighted data rather than fa. In: Proceedings of the International Society of Magnetic Resonance in Medicine, p. 2018.
- Hagmann, P., Thiran, J.P., Jonasson, L., Vandergheynst, P., Clarke, S., Maeder, P., Meuli, R., 2003. DTI mapping of human brain connectivity: statistical fiber tracking and virtual dissection. NeuroImage 19, 545–554.
- Hall, M.G., Alexander, D.C., 2009. Convergence and parameter choice for Monte-Carlo simulations of diffusion MRI. IEEE Transactions on Medical Imaging 28, 1354–1364.
- Hubbard, P.L., Parker, G.J., 2009. Validation of tractography. In: Behrens, T.E.B., Johansen-Berg, H. (Eds.), Diffusion MRI. Elsevier.
- Iturria-Medina, Y., Sotero, R.C., Canales-Rodriguez, E.J., Alemàn-Gòmez, Y., Melie-Garcia, L., 2008. Studying the human brain anatomical network via diffusionweighted mri and graph theory. NeuroImage 40, 1064–1076.
- Jbabdi, S., Woolrich, M., Andersson, J., Behrens, T., 2007. A bayesian framework for global tractography. NeuroImage 37, 116–129.
- Jones, D.K., Knösche, T.R., Turner, R., 2013. White matter integrity, fiber count, and other fallacies: the do's and don'ts of diffusion MRI. NeuroImage 73, 239–244. http://dx.doi.org/10.1016/j.neuroimage.2012.06.081.
- Kezele, I., Descoteaux, M., Poupon, C., Poupon, F., Mangin, J.F., 2010. Spherical wavelet transform for odf sharpening. Medical Image Analysis 14, 332–342.
- Kinoshita, M., Yamada, K., Hashimoto, N., Kato, A., Izumoto, S., Baba, T., Maruno, M., Nishimura, T., Yoshimine, T., 2005. Fiber-tracking does not accurately estimate size of fiber bundle in pathological condition: initial neurosurgical experience using neuronavigation and subcortical white matter stimulation. Neuroimage 25, 424–429.
- Kreher, B.W., Mader, I., Kiselev, V.G., 2008. Gibbs tracking: a novel approach for the reconstruction of neuronal pathways. Magnetic Resonance in Medcine 60, 953– 963.

- Kreher, B.W., Schneider, J.F., Mader, J., Martin, E., Hennig, J., Il'yasov, K., 2005. Multitensor approach for analysis and tracking of complex fiber configurations. Magnetic Resonance in Medicine 54, 1216–1225.
- Lazar, M., Weinstein, D., Tsuruda, J., Hasan, K., Arfanakis, K., Meyerand, M., Badie, B., Rowley, H., Haughton, V., Field, A., Alexander, A., 2003. White matter tractography using diffusion tensor deflection. Human Brain Mapping 18, 306–321.
- Leergaard, T.B., White, N.S., deCrespigny, A., Bolstad, I., D'Arceuil, H., Bjaalie, J.G., Dale, A.M., 2010. Quantitative histological validation of diffusion MRI fiber orientation distributions in the rat brain. PloS One 5, e8595.
- Michailovich, O.V., Rathi, Y., 2009. On approximation of orientation distributions by means of spherical ridgelets. IEEE Transactions on Image Processing 19, 461– 477.
- MomayyezSiahkal, P., Siddiqi, K., 2010. Probabilistic anatomical connectivity using completion fields. In: International Conference on Medical Image Computing and Computer Assisted Intervention (MICCAI'10), pp. 566–573.
- Mori, S., Crain, B.J., Chacko, V.P., Van Zijl, P.C.M., 1999. Three-dimensional tracking of axonal projections in the brain by magnetic resonance imaging. Annals of Neurology 45, 265–269.
- Moussavi-Biugui, A., Stieltjes, B., Fritzsche, K., Semmler, W., Laun, F., 2011. Novel spherical phantoms for q-ball imaging under in vivo conditions. Magnetic Resonance in Medicine 65, 190–194.
- Nedjati-Gilani, S., Geoff, D.C.A., Parker, J.M., 2008. Regularized super-resolution for diffusion mri. In: IEEE International Symposium on Biomedical Imaging: from Nano to Macro, pp. 875–878.
- Özarslan, E., Shepherd, T., Vemuri, B., Blackband, S., Mareci, T., 2006. Resolution of complex tissue microarchitecture using the diffusion orientation transform (dot). NeuroImage 31, 1086–1103.
- Parker, G.J.M., Haroon, H.A., Wheeler-Kingshott, C.A.M., 2003. A framework for streamlinebased probabilistic index of connectivity (pico) using structural interpretation of mri diffusion measurements. Journal Magnetic Resonance Imaging 18, 242–254.
- Péchaud, M., Descoteaux, M., Keriven, R., 2009. Brain connectivity using geodesics in HARDI. In: Proceeedings of Medical image computing and computer-assisted intervention (MICCAI), London, United Kingdom, pp. 482–489.
- Perrin, M., Poupon, C., Cointepas, Y., Rieul, B., Golestani, N., Pallier, C., Riviere, D., Constantinesco, A., Bihan, D.L., Mangin, J.F., 2005. Fiber tracking in q-ball fields using regularized particle trajectories. In: Proceedings of Information Processing in Medical, Imaging, pp. 52–63.
- Pontabry, J., Rousseau, F., 2011. Probabilistic tractography using Q-ball modeling and particle filtering. Medical image computing and computer-assisted intervention: MICCAI. International Conference on Medical Image Computing and Computer-Assisted Intervention 14, 209–216.
- Poupon, C., Laribiere, L., Tournier, G., Bernard, J., Fournier, D., Fillard, P., Descoteaux, M., Mangin, J.F., 2010. A diffusion hardware phantom looking like a coronal brain slice. In: Proceedings of the International Society for Magnetic Resonance in Medicine.
- Poupon, C., Rieul, B., Kezele, I., Perrin, M., Poupon, F., Mangin, J.F., 2008. New diffusion phantoms dedicated to the study and validation of hardi models. Magnetic Resonance in Medicine 60, 1276–1283.
- Pullens, P., Roebroeck, A., Goebel, R., 2010. Ground truth hardware phantoms for validation of diffusion-weighted MRI applications. Journal of Magnetic Resonance Imaging; JMRI 32, 482–488.
- Raffelt, D., Tournier, J.D., Rose, S., Ridgway, G.R., Henderson, R., Crozier, S., Salvado, O., Connelly, A., 2012. Apparent fibre density: a novel measure for the analysis of diffusion-weighted magnetic resonance images. NeuroImage 59, 3976–3994.

- Reisert, M., Mader, I., Anastasopoulos, C., Weigel, M., Schnell, S., Kiselev, V., 2011. Global fiber reconstruction becomes practical. NeuroImage 54, 955–962.
- Röttger, D., Seib, V., Müller, S., 2011. Distance-based tractography in high angular resolution diffusion MRI. The Visual Computer 27, 729–738.
- Scherrer, B., Gholipour, A., Warfield, S.K., 2012. Super-resolution reconstruction to increase the spatial resolution of diffusion weighted images from orthogonal anisotropic acquisitions. Medical Image Analysis 16, 1465–1476.
- Sepasian, N., ten Thije Boonkkamp, H., Vilanova, A., ter Haar Romeny, B., 2009. Multi-valued geodesic based fiber tracking for diffusion tensor imaging. In: MICCAI Workshop on Computational Diffusion MRI (CDMRI), London, United Kingdom, pp. 148–158.
- Seunarine, K.K., Alexander, D., 2009. Multiple fibres: beyond the diffusion tensor. In: Behrens, T.E.B., Johansen-Berg, H. (Eds.), Diffusion MRI. Elsevier.
- Smith, R.E., Tournier, J.D., Calamante, F., Connelly, A., 2012a. Anatomicallyconstrained tractography: improved diffusion MRI streamlines tractography through effective use of anatomical information. NeuroImage 62, 1924–1938.
- Smith, R.E., Tournier, J.D., Calamante, F., Connelly, A., 2012b. Structurally-informed tractography: improved diffusion MRI streamlines tractography using anatomical information. In: International Symposium on, Magnetic Resonance in Medicine (ISMRM'12), p. 1907.
- Sotiropoulos, S.N., 2010. Processing of diffusion-weighted MR images of the brain: from crossing fibres to distributed tractography. Ph.D. thesis, University of Nottingham.
- Spena, G., Nava, A., Cassini, F., Pepoli, A., Bruno, M., DAgata, F., Cauda, F., Sacco, K., Duca, S., Barletta, L., Versari, P., 2010. Preoperative and intraoperative brain mapping for the resection of eloquent- area tumors: a prospective analysis of methodology, correlation, and usefulness based on clinical outcomes. Acta Neurochirurgica 152, 1835–1846.
- Tournier, J.D., Calamante, F., Connelly, A., 2007. Robust determination of the fibre orientation distribution in diffusion mri: non-negativity constrained superresolved spherical deconvolution. NeuroImage 35, 1459–1472.
- Tournier, J.D., Calamante, F., Connelly, A., 2011. Effect of step size on probabilistic streamlines: implications for the interpretation of connectivity analyses. In: International Symposium on Magnetic Resonance in Medicine (ISMRM'11), p. 2019.
- Tournier, J.D., Calamante, F., Connelly, A., 2012. MRtrix: diffusion tractography in crossing fiber regions. International Journal of Imaging Systems and Technology 22, 53–66.
- Tristán-Vega, A., Aja-Fernández, S., 2010. Dwi filtering using joint information for dti and hardi. Medical Image Analysis 14, 205–218.
- Tuch, D., 2004. Q-ball imaging. Magnetic Resonance in Medicine 52, 1358–1372.
- Weinstein, D., Kindlmann, G., Lundberg, E., 1999. Tensorlines: advection-diffusion based propagation through diffusion tensor fields. In: Proceedings Visualization '99, vol. 3, pp. 249–530.
- Wilkins, B., Lee, N., Nam, K., Hwang, D., Singh, M., 2012a. Comparison of novel ICAbased approach to existing diffusion MRI multi-fiber reconstruction methods. In: International Symposium on Magnetic Resonance in Medicine (ISMRM'12), p. 1934.
- Wilkins, B., Lee, N., Singh, M., 2012b. Development and evaluation of a simulated FiberCup phantom. in: International Symposium on Magnetic Resonance in Medicine (ISMRM'12), p. 1938.
- Wu, J., Zhou, L., Tang, W., Mao, Y., Hu, J., Song, Y., Hong, X., Du, G., 2007. Clinical evaluation and follow-up outcome of diffusion tensor imaging-based functional neuronavigation: a prospective, controlled study in patients with gliomas involving pyramidal tracts. Neurosurgery 61, 935–949.